Cerebral embolic protection during endovascular arch replacement

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Despite excellent results in high volume centers, open repair of aortic arch pathology is highly invasive, and can result in significant morbidity and mortality in high risk patients. Near-total and hybrid approaches to aortic arch disease states have emerged as an alternative for patients deemed moderate to high risk for conventional repair. Advantages of these approaches include avoidance of extracorporeal circulation and hypothermic circulatory arrest as well as avoidance of cross clamping, all of which are not well tolerated in high risk patients. Anatomically high-risk patients with anastomotic aneurysms from previous arch reconstruction may also benefit from these less invasive approaches. Medical devices designed specifically for the aortic arch are developing at a rapid pace and continue to evolve. Dedicated devices for zone 0–2 aortic arch repair are currently available under special access or being studied in clinical trials. Unfortunately, stroke continues to be the Achilles heel of endovascular approaches to the aortic arch, with cerebral embolism being the culprit in the majority of such cases. This perspective article describes the epidemiology, and specifically addresses current means of embolic protection and future direction.

Keywords: Arch; endovascular; stroke; embolism; protection



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Introduction

One of the most devastating complications after cardiac surgery is stroke. Conventional open repair of aortic arch pathology is highly invasive and frequently requires extracorporeal circulation and hypothermic circulatory arrest, both sources of stroke. Despite advances in perioperative management and surgical technique, contemporary series of aortic arch repair report a significant risk of stroke (4.7–6.0%) (1,2).

Near-total endovascular repair of aortic arch pathology, and hybrid approaches that combine surgical revascularization of the brachiocephalic arteries with thoracic endovascular aortic repair (TEVAR) have appeared as promising alternatives. Although these approaches can mitigate risk associated with cardiopulmonary bypass, circulatory arrest, and aortic cross clamping, strokes after endovascular procedures of the arch still contribute a significant risk to the patient with rates of 4.2-5.9%(*Table 1*) (3-5). Mechanisms of stroke include embolism or aortic dissection with wire and catheter manipulations, and during deployments of endografts, in addition to cerebral hypoperfusion during revascularization of the supra-aortic trunks. Sources of emboli may include fresh or organized thrombus, atheromatous debris, air, or native arterial tissue. Several strategies exist to mitigate stroke risk during endovascular approaches to the arch. However, new innovations in device design constantly introduce new

Table 1 Rates of neurological events and mortality associated with different techniques of aortic arch repair							
First author, year	n	PLZ	Technique	Perioperative mortality (%)	Cerebral ischemic events (%)	Stroke (%)	TIA (%)
Thomas, 2012 (1)	209	N/A	Open arch replacement	4.3	6.7	6.2	0.5
Patel, 2011 (2)	721	N/A	Open arch replacement	5.0	4.7	4.7	NR
Melissano, 2012 (3)	32	0	Hybrid repair	9.4	49.4	9.4	NR
	35	1	Hybrid repair	2.8	0	0	NR
	76	2	Hybrid repair	2.6	1.4	1.4	NR
Feezor, 2007 (4)	80	0–2	Hybrid repair	NR	9	9	NR
	116	3–4	Hybrid repair	NR	2	2	NR
Andrasi, 2017 (5)	429	0–3	Open debranching	NR	7.5	NR	NR
	190	0–3	Partial endovascular	NR	11	NR	NR
	402	0–3	Totally endovascular	NR	1.74	NR	NR
Waterford, 2016 (6)	824	2	TEVAR alone, no LSA revascularization	NR	5.6	5.6	NR
	413	2	TEVAR with LSA revascularization	NR	3.1	3.1	NR
Moulakakis, 2013 (7)	956	0–2	Hybrid repair	11.9	7.6	NR	NR
Czerny, 2012 (8)	66	0	Hybrid repair	9	5	5	NR
Antoniou, 2010 (9)	195	0–1	Hybrid repair	9	7	7	NR
Preventza, 2015 (10)	274	N/A	Open arch replacement	10	5.5	5.5	NR
	45	0	Hybrid repair	11	9	9	NR
Yoshitake, 2016 (11)	23	0	Multiple techniques*				
	28	1	Hybrid repair				
	23	2	Hybrid repair				
Inoue, 1999 (12)	1	0	Triple-branched TEVAR	0	0	0	NR
	14	2	Single-branched TEVAR	0	7	7	NR
lwakoshi, 2015 (13)	32	0–1	Fenestrated TEVAR	0	3	3	NR
Haulon, 2014 (14)	38	0	Inner branched TEVAR	13.2	13	3	10.5
Spear, 2016 (15)	27	0	Inner branched TEVAR	0	11	11	0
Patel, 2016 (16)	22	2	Single-branched TEVAR	0	0	0	NR

*, complete arch debranching (n=11), innominate artery chimney graft with axillo-axillary and left common carotid artery bypass (n=5), or fenestrated stent graft with extra-anatomic bypasses (n=7). PLZ, proximal landing zone; NR, not reported; TEVAR, thoracic endovascular aortic repair; LSA, left subclavian artery; TIA, transient ischemic attack.



Figure 1 University of Pennsylvania classification of hybrid aortic arch repair [used with permission from Vallabhajoysula et al. (22)].

challenges in stroke reduction.

Epidemiology of stroke in arch endovascular procedures

Stroke risk during arch TEVAR varies with both the method and extent of repair. With rapidly developing endovascular technology for treatment of arch pathology, elucidating rates and causes of peri-operative stroke has been difficult. Challenging arch anatomy, advancing devices and wires proximally into the aortic arch and ascending aorta, and complexity of the procedure all contribute to the differences in stroke rates. A greater understanding of the epidemiology of stroke can assist in anticipation and avoidance of stroke in endovascular approaches to arch pathology.

Atheromatous disease

Aortic arch atherosclerosis is commonly found in the population and can contribute to embolic phenomena. In the SPARC study, 51% of the population over the age of \geq 45 years had the presence of arch atheroma with 7.6% having severe atheroma as defined by \geq 4 mm thick, ulcerated or mobile plaque (17). The presence of severe arch atheroma increases with age and is found in over 20% of patients \geq 75 years.

Several studies of TEVAR for distal arch or descending aortic pathology have demonstrated an association of

significant arch atheroma/shaggy aorta and peripheral embolization with stroke (18-21).

Hybrid approaches

When hybrid arch repair involves proximal arch landing zones, surgical debranching is required to maintain cerebral perfusion when the endograft is expected to exclude the supra-aortic vessels. Hybrid approaches have the benefit of combining a more limited, less invasive open revascularization with a relatively straightforward endovascular procedure. Although many configurations of hybrid approaches exist, the University of Pennsylvania group classified hybrid approaches into a practical classification that includes three types of repair (Figure 1) (22). Type I includes a ortic debranching using a partial aortic clamp and a zone 0 landing zone, completely avoiding cardiopulmonary bypass. Type II requires surgical construction of a zone 0 landing zone requiring cardiopulmonary bypass and often circulatory arrest. Type III hybrid approaches include full reconstruction of the ascending aorta and arch. Further expansion of this classification can include arch reconstruction at zone 1 or 2. Selected strategies are tailored to patient anatomy.

Stroke rates in hybrid repairs are influenced by crossclamping, clamping of branches vessels, hypoperfusion, circulatory arrest, and endovascular manipulations.

Major strokes occurred during hybrid repair for zone 0 or zone 1 pathology in 4.7–9.5% (11) of patients (3,6-10).

Although robust data for stroke rates at each zone is sparse, higher stroke rates seem to correspond with more proximal debranching with zone 0, zone 1, and zone 2 hybrid repair stroke rates being 17.4%, 7.1%, and 4.3%, respectively (11).

Procedures with increased wire manipulation

Repair with fenestrated/branched endografts

Fenestrated and branched endografts for the aortic arch were developed as a means to achieve near total endovascular repair of the arch, eliminating most of the debranching required with hybrid repair. The majority of the global experience with branched arch endografts is with the Cook Medical Zenith arch branched graft (Bloomington, IN, USA), a two-branch device developed for proximal sealing in zone 0. All patients undergo left subclavian artery (LSA) revascularization and the branches are bridged to their target vessels (innominate and left common carotid) with an appropriate covered bridging stent graft. The initial global experience of 38 patients treated with this device was reported in 2014 in patient who were deemed high-risk or unfit for conventional surgery. Stroke, transient ischemic attack (TIA) and meningeal hemorrhage occurred in six patients (15.7%) (14). A more recent study using the same device in high risk patients reported two major strokes among 27 patients treated (7.4%) (15). The authors concluded that decreased stroke rate was directly correlated with the learning curve involved with these complex novel procedures.

Arch endografts with multiple fenestrations or branches [Nexus (Endospan Ltd., Herzlia, Israel); arch branch graft (Cook Medical); arch branched stent graft (Bolton Medical Inc., Sunrise, Florida, USA)] (Figure 2) are not currently commercially available in the United States, and are generally only available worldwide under special or compassionate use access although plans are underway for feasibility clinical trials in the United States the Gore TAG Thoracic Branch Endoprosthesis (W.L. Gore, Flagstaff, AZ, USA), a single branch device (Figure 2), is currently undergoing a US pivotal clinical trial. While this pivotal trial has recently been opened up to zone 0 and 1 pathology, the initial results of repair in zone 2 (Gore TAG TBE feasibility trial) were published, demonstrating no strokes in 22 patients treated (16). Medtronic has recently restarted their feasibility trial examining safety and efficacy of their Mona LSA branch stent graft system, with a single "Volcano" like branch intended for zone 2 cases (Figure 2). The high-risk nature of the patients,

increased wire and catheter manipulation in the branch vessels and arch, and deployment of branch devices and balloons in the branch vessels all contribute to stroke risk in these patients.

Repair with parallel grafts

Parallel chimney stents were initially conceived as a bailout maneuver in cases of inadvertent visceral artery coverage during endovascular abdominal aortic repair, but the technique has since been extended to other applications (23). It has been used widely in the paravisceral aorta and is increasingly being used to manage the supra-aortic branches during TEVAR. Briefly, a covered stent runs in parallel to the aortic endoprosthesis into the branch vessel and serves as a bridge from the aorta, within the seal zone, to the vessel that has been intentionally covered. The principal advantage of this off label technique is in its use of off-theshelf components and techniques familiar to most operators to achieve a more proximal landing zone during arch TEVAR. The disadvantage of this technique is the creation of gutters around the aortic endoprosthesis with a 6.4–9.4% rate of type IA endoleak (24,25).

The rate of major stroke during chimney TEVAR was 2.6–5.4% (20,25). In Hogendoorn *et al.*, 24% of patients who underwent arch chimney grafts required an additional cervical debranching procedure; the stroke rate in these patients was 8.3% versus 3.2% for those who did not have additional revascularization, with 40% of strokes being fatal (25).

Implantation of chimney grafts requires more wire and catheter manipulations within the arch compared to TEVAR with debranching, and these manipulations in and around the arch vessels may contribute to cerebral embolization.

LSA coverage

In order to achieve a more stable and reliable proximal landing zone, or as part of proximal arch procedures, the LSA will often require endovascular occlusion. Stroke rates of 4.8–7.4% have been reported in patients undergoing TEVAR with LSA coverage (6). The Eurostar registry has identified LSA coverage as significantly associated with higher neurological sequelae (26). Coverage of the LSA with and without revascularization demonstrated lower risk of stroke in patients who had LSA revascularization (5.3% 95% CI: 2.6–8.6 vs. 8.0% 95% CI: 4.1–12.4) (17); and 3.1% vs. 5.6%, P=0.0657 (6). We recommend LSA revascularization whenever feasible.



Figure 2 Aortic arch stent graft devices in different phases of development. (A,B) Cook Zenith arch branched device (Cook Medical LLC, Bloomington, Indiana, USA); (C) Gore TAG Thoracic Branch Endoprosthesis (W. L. Gore & Associates, Inc., Flagstaff, Arizona, USA); (D) Bolton Relay arch branched stent graft (Bolton Medical Inc, Sunrise, Florida, USA); (E) Medtronic Valiant Mona LSA (Medtronic PLC, Minneapolis, Minnesota, USA); (F) Endospan Nexus stent graft (Endospan Ltd., Herzlia, Israel).

Techniques at minimizing stroke

Pre-operative planning

The planning phase of arch endovascular therapy remains an essential step in stroke minimization. Anticipating and avoiding potential sources of stroke is likely the best strategy in stroke prevention.

Imaging

Identifying potential embolic sources on chest CTA imaging can alter pre-operative planning as well as intraoperative strategies. Calcific disease, atheroma, dissection flaps, and ulcerations can all contribute to embolic phenomena and strategies aimed at avoiding or excluding these zones from circulation are ideal. Knowledge of the presence and dominance of vertebral artery circulation is required for subclavian artery revascularization options, and head and neck imaging are strongly recommended to establish circle of Willis anatomy. Branch origin disease, tortuosity, and arch elongation can contribute to technical challenges in advancing and positioning devices in the ascending aorta, branch vessels, and arch. Anticipating these challenges can minimize wire manipulations and failed attempts at advancing devices, thus reducing risk of stroke.

ECG-gated computed tomography angiography is the ideal imaging modality for arch planning. Gating, whether

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prospective ECG triggered or retrospective ECG, improves temporal resolution and minimizes artifacts caused by cardiac motion (27) allowing for accuracy in measurement. Uploading images into 3D software for measurement is highly recommended.

Device selection

The anatomical constraints of the ascending aorta and arch can be extremely unforgiving in the endovascular setting. Arch configuration and aortic tortuosity (proximal or distal) can contribute to challenges in advancing wires, catheters, and devices without 'snowplowing' the aortic wall. When these situations are encountered, the most important step in stroke minimization is selecting the proper approach to managing the aortic pathology. In highly angulated or elongated arches, total arch endovascular techniques may carry high stroke risk compared to hybrid techniques and when atheromatous burden is high endovascular manipulations in the high-risk arch may be better avoided, preferring a completely open strategy. When selecting which device or strategy to employ for arch pathology, device conformability, stiffness of the delivery system, and operator familiarity should all be considered.

Intra-operative techniques

Wires and catheters

Proper wire and catheter use represents best clinical practice in stroke reduction. Prior to advancing any wires across the arch, adequate heparinization with 100–200 units/kg of Heparin with a goal ACT of >250 must be achieved. Furthermore, it is recommended that American Society of Anesthesiologists Physical Status Classification System (ASA) and, selectively, clopidogrel be continued throughout the procedure.

Wires should never be advanced without fluoroscopic visualization. Whenever possible, standardizing wire and catheter selection to minimize unnecessary exchanges is advisable. The decision to position the wire in the ascending aorta or in the left ventricle, ideally should be determined pre-procedurally. Careful attention to marking and stabilizing these wires is essential. If advanced wire techniques are necessary such as through and through wire access, snaring should be performed distal to the arch to avoid inadvertent cerebral embolization.

Device manipulation

When anatomical constraints present challenges in device

delivery or deployment, the operator must move quickly to alternate techniques, abandoning multiple or forced ineffective attempts. Stiff buddy wires and through and through wire access (brachial/subclavian/axillary) can provide the support needed to navigate tortuous anatomy and safely advance delivery systems into the proximal aorta. These techniques can be planned in challenging anatomy. Iliac and aortic tortuosity is often underestimated as a possible cause of inability to introduce the device into the arch. Pre-planning is often beneficial to countering these challenges and alternative access options such as iliac conduits or direct abdominal aortic access can circumvent these obstacles.

Adjunctive procedures and devices

LSA revascularization

When feasible, we strongly recommend routine carotidsubclavian bypass or transposition of the LSA, in order to minimize stroke and spinal injury. If lengthy endovascular procedures are planned, LSA revascularization is performed in a staged fashion the day prior.

Embolic protection devices (EPD)

There is a paucity of data regarding techniques or devices for embolic protection for use during arch TEVAR. Experience with methods for prevention of embolization has been gained in other endovascular procedures at risk for cerebral embolization, specifically in internal carotid artery stenting (CAS) and transcatheter aortic valve replacement (TAVR).

The most commonly used EPD are distal filters with occlusion/aspiration systems used less commonly (28). Distal filter EPDs are deployed over a 0.014" wire or come attached to a steerable wire tip and allow antegrade carotid blood flow during the entirety of the procedure, real-time capture of embolic debris, and angiography at any time during the intervention. In CAS, use of EPDs has demonstrated a significant reduction in both minor stroke (0.5% vs. 3.7%; P<0.001) and major stroke (0.3% vs. 1.1%; P<0.05) (29) and are currently in widespread use for this application.

Various EPDs have been studied in the setting of TAVR. The Claret Sentinel device (Claret Medical Inc., Santa Rosa, California, USA) consists of a dual-filter system inserted through a 6 French sheath inserted via right arm access. The proximal component, a radiopaque nitinol frame with a 140-µm pore polyurethane filter, is deployed in the IA



Figure 3 FilterWire EZ[™] Embolic Protection System (Boston Scientific Corporation, Marlborough, Massachusetts, USA).

and a second filter is positioned across the left common carotid artery (LCCA) ostium. This device protects the right vertebral, right carotid, and left carotid arteries from embolization but not the left vertebral. Conversely, the TriGuard HDH embolic deflection device (Keystone Heart Ltd., Caesarea, IL, USA) is delivered transfemorally via a 9 French Mullins introducer sheath and deploys a single mesh filter with 130-µm pores across the ostia of all three head vessels. These devices demonstrated significantly decreased risk of stroke in patients undergoing TAVR procedures (30,31). Disadvantages of these EPDs include the requirement of an additional arterial access (up to 9 French in the case of the TriGuard), lack of protection of the left vertebral artery by the Sentinel device, and availability of only one size for each device leading to incomplete coverage in certain arch anatomies. Variability in arch anatomy and the wide spectrum of possible arch pathologies makes no single embolic protection device or technique applicable to all situations or repair techniques. Diversion/filtering devices used for TAVR pose a technical challenge for embolic protection during zone 0-2 arch repair compared to when they are used during TAVR as they are likely to interfere with the deployment of the aortic endoprosthesis. If still in place once the TEVAR is implanted, removal of the EPD could potentially displace the endoprosthesis or more importantly result in entrapment of the EPD. Two additional EPD devices, the Embol-X and Embrella devices did not demonstrate reduction in the incidence of large total lesion volume. The Embol-X device study was stopped before completion due to commercial unavailability of the device, and studies of the Embrella device were not powered for efficacy, and actually trended towards an increase in lesion numbers (32). Neither of these devices are commercially available in the United States.

The senior author has used the Boston Scientific FilterWire EZ (*Figure 3*) EPD in four cases of advanced aortic arch intervention. These devices are intended for transfemoral placement into the mid internal carotid artery. This method of use is contraindicated for arch branched cases due to the device being entrapped by the full deployment of the arch branched graft. Therefore, if one intends to use these neuroprotective devices, they must be placed via direct access of the supra-aortic vessels. On the right, direct mid to distal common carotid access is required, and for left internal carotid deployment, the device is introduced by way of the left carotid subclavian bypass usually by direct puncture in the synthetic graft. Direct access as described above can be cumbersome and awkward with the long delivery systems of the EPD being exposed to possible inadvertent manipulations and credible fear that the EPD could be dragged back on an exposed internal carotid artery. Even more worrisome is the concern for the 0.014" delivery wire being bent or kinked while distracted by the other manipulations of the arch branched graft or the supra aortic access. Clearly, if carotid neuroprotection is desired using this modality, development of a more procedure-specific neuroprotection device is required. Interestingly, despite the use of direct neuroprotection with EPD in the internal carotid artery, one out of these four patients experienced a significant stroke. Examination of the filter in that case demonstrated significant debris in the filter, confirming the very real possibility of embolic potential in these complex arch cases (Figure 4).

Carotid clamping

Clamping and flushing of the carotid vessels is a relatively simple method of embolic protection. It can be considered when stroke risk is high secondary to excessive atheromatous burden in the ascending aorta and arch. This technique is limited by a few different variables: not all vessels are surgically exposed in every case; clamping of the artery itself may cause embolization in the cases of diseased arteries; and cerebral hypoperfusion can occur. In general, surgeons experienced with clamping currently favor the technique of sequential clamping of the common carotid artery distal to the retrograde catheterization point while the branch intervention is performed, with subsequent flushing before opening the carotid to antegrade flow. This of course is predicated by adequate collateral flow via a patent circle of Willis, along with systemic blood pressure that supports this robust cerebral network. We routinely maintain systemic blood pressure in the normotensive or hypertensive during range during carotid clamping to



Figure 4 FilterWire EZ[™] Embolic Protection System (Boston Scientific Corporation, Marlborough, Massachusetts, USA) containing embolic debris captured during an branched aortic arch endovascular repair.

minimize the risk of hypoperfusion.

Conclusions

Many factors can contribute to the risk of stroke during endovascular therapy to arch pathology. Approaches to the arch whether open, near-total endovascular, or hybrid, all carry different risk of stroke but must be individualized to the patient in order to achieve the best outcomes with the lowest risk of peri-operative mortality and stroke. Patient factors such as arch atheroma and ulceration, and arch elongation, are not modifiable and must be identified early and be strategically considered during the planning phase. Currently, there are no neuroprotection devices available that are specifically compatible with endovascular repair of arch pathology. Techniques in stroke prevention such as carotid clamping and/or EPD placed directly through supraaortic vessels should be considered when appropriate, on an individual basis. Sound clinical practice such as diligence with wire and device manipulations is always recommended. As endovascular therapy continues to push the boundaries of aortic arch management, the cause and prevention of strokes will continue to evolve. There is clearly opportunity and need for innovation in neuroprotection for complex endovascular arch intervention. Until this need is met, stroke will continue to be the Achilles heel of endovascular aortic arch intervention.

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Footnote

Conflicts of Interest: Dr. Cherrie Abraham is a Consultant for Cook Medical (Case reviews, Proctoring Advanced Aortic Intervention), Medtronic (Aortic Advisory Board), and WL Gore (Clinical Events Committee, Gore Clinical Trial)— (Consultant fees paid to OHSU). The other authors have no conflicts of interest to declare.

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